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4 Committee for Medicinal Products for Veterinary use (CVMP)  
5 Quality Working Party (QWP)  
6 Biologics Working Party (BWP)

7 **Guideline on the sterilisation of the medicinal product,**  
8 **active substance, excipient and primary container**  
9 **Draft**

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10  
11 This guideline replaces Decision trees for the selection of sterilisation methods (CPMP/QWP/054/98),  
12 the Annex to the note for guidance on development pharmaceuticals (CPMP/QWP/155/96); and  
13 The Annex "Decision trees for the selection of sterilisation methods" (EMA/CVMP/065/99) to the note  
14 for guidance: Development pharmaceuticals for veterinary medicinal products (EMA/CVMP/315/98).

15  
16 Comments should be provided using this [template](#). The completed comments form should be sent to  
QWP@ema.europa.eu

<b>Keywords</b>	Active substance, Aseptic processing, Container, Decision trees, Excipients, Filtration, Finished Dosage form, Sterilisation, Sterilisation assurance level, Terminal sterilisation
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17 **Guideline on sterilisation of the medicinal product, active**  
18 **substance, excipient and primary container**

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## 32 **Executive summary**

33 This guideline provides guidance on the documentation expected for sterile products in the quality  
34 dossier for a marketing authorisation application or a variation application for a medicinal product,  
35 (called quality dossier throughout the guideline), and the selection of appropriate methods of  
36 sterilisation for sterile products. Although, terminal sterilisation using a reference condition of the  
37 European Pharmacopoeia (Ph. Eur) is the method of choice whenever possible, this guideline provides  
38 information on when other terminal sterilisation processes, sterilising filtration or aseptic processing,  
39 (either alone or when combined with an additional terminal microbial reduction process), could be  
40 accepted as an alternative to a reference terminal sterilisation process.

41 This guideline replaces the previous Annexes to Pharmaceutical development *Decision trees for the*  
42 *selection of sterilisation methods*, (human and veterinary). In addition, the information on methods of  
43 sterilisation previously described in *Note for Guidance on manufacture of the finished dosage form*  
44 (human and veterinary) has been revised and included in this guideline.

## 45 **1. Introduction (background)**

46 Sterility is a critical quality attribute for all sterile products. Sterility of the medicinal product cannot be  
47 assured by testing, it needs to be assured by the use of a suitable and validated manufacturing  
48 process. Sterility is dependent on several factors such as the bioburden of the formulation  
49 components, the sterilisation procedure, the integrity of the container closure system, (abbreviated as  
50 container in this document), and in the case of aseptic processing, the use of satisfactory aseptic  
51 technique. Container integrity is discussed in ICH Q8, (formally adopted for human medicinal products  
52 only, nevertheless the same principles are also applicable to veterinary medicinal products).

53 Terminal sterilisation is preferred to sterilisation by filtration and/or aseptic processing because it  
54 provides a sterility assurance level (SAL) that is possible to calculate, validate and control, and thus  
55 incorporates a safety margin. For aseptic processes, a SAL is not applicable as accidental  
56 contamination caused by inadequate technique cannot be reliably eliminated by monitoring, control or  
57 validation. Therefore, terminal sterilisation provides the highest assurance of sterility and should be  
58 used whenever possible. For highly sensitive products such as biological products where terminal  
59 sterilisation of the drug product is not possible, aseptic processing under controlled conditions provides  
60 a satisfactory quality of the drug product.

61 In addition to those products where the formulation itself prohibits the possibility of terminal  
62 sterilisation, the use of aseptic processing can be accepted in certain situations even if the formulation  
63 itself can be terminally sterilised if other benefits are gained for the patients or users of the product.  
64 These situations are specified below in section 4.3.

## 65 **2. Scope**

66 The guideline applies to chemical and biological medicinal products for human and veterinary use, but  
67 is not applicable for immunological veterinary medicinal products.

68 Guidance is provided on the choice of the method of sterilisation, the development and manufacturing  
69 data required to support the manufacture of the finished product. The same principles, (choice of  
70 method of sterilisation, development data and manufacturing), apply to sterile active substances,  
71 excipients and primary containers. Only the information expected in a quality dossier, including  
72 information on the need for Good Manufacturing Practice (GMP) certificates, is described. General GMP  
73 requirements are not included.

74 Terminal sterilisation by heat and ionising irradiation, using the reference conditions of Ph. Eur. 5.1.1  
75 “Methods of preparation of sterile products” or other conditions to achieve a SAL of  $\leq 10^{-6}$ , sterilisation  
76 by filtration and aseptic processing are considered. Terminal sterilisation by gas and its limitations is  
77 also addressed.

78 The concepts in this guideline refer only to absence or removal of bacteria and fungi. The absence,  
79 removal or inactivation of viruses, mycoplasma and other adventitious agents, which could  
80 contaminate a product, are not considered.

### 81 **3. Legal basis**

82 This guideline should be read in conjunction with Directive 2001/83/EC on the community code relating  
83 to medicinal products for human use Directive 2001/82/EC on medicinal products for veterinary use as  
84 amended and also the current Ph. Eur.

85 In addition, this guideline should be read in conjunction with all other relevant directives and  
86 regulations, and all relevant Commission, (V)ICH and CXMP guidelines, Q&A documents and other  
87 documents as linked to or published on the EMA website ([www.ema.europa.eu](http://www.ema.europa.eu)).

### 88 **4. General requirements**

89 The guideline concerns only specific requirements relating to sterility and sterile products. For other  
90 considerations on the manufacturing of the medicinal product, reference is made to other guidance  
91 documents such as Guidelines on Manufacture of the Finished Dosage Form.

#### 92 ***4.1. Manufacturing of sterile medicinal products***

93 Documentation regarding sterilisation and aseptic processing to be included in the quality dossier,  
94 Module 3, sections 3.2.P.2 Pharmaceutical development and 3.2.P.3 Manufacture for human products  
95 or Part 2 A.4 Development pharmaceuticals and Part 2 B Description of the manufacturing method for  
96 veterinary products is presented below. The documentation should be provided for all sites performing  
97 sterilisation or aseptic processing related to the medicinal product, regardless of whether the processes  
98 are performed in-house or outsourced.

99 The choice of method of sterilisation or aseptic processing should be justified, see section 4.3 Selection  
100 of sterilisation method.

101 All sterilisation processes should be carried out according to the instructions of the Ph. Eur. unless  
102 justified.

103 All sterilisation procedures for the active substance, the excipient(s) or the primary containers should  
104 be described and the name and address of the site responsible should be stated. Validation data should  
105 be provided as described below for each sterilisation process. The required validation data for terminal  
106 microbial reduction processes is the same as for the sterilisation processes, except for the  
107 demonstration of a SAL of  $10^{-6}$  or better.

108 When parametric release of sterility is proposed, the Guideline on real time release testing (formerly  
109 Guideline on parametric release), EMA/CHMP/QWP/811210/2009-Rev1 (human products only), the  
110 Guideline on Parametric release, EMEA/CVMP/QWP/339588/2005 (veterinary products only) and the  
111 text of Ph. Eur. Chapter 5.1.1 should be taken into account.

112 The levels of bioburden and bacterial endotoxins in the components (active substance, excipients and  
113 primary package), as well as those introduced during manufacture and sterilisation can have an impact  
114 on the level of bacterial endotoxins in the finished drug product. To ensure an acceptable level of  
115 bacterial endotoxins in the finished drug product, the microbiological contamination of the components  
116 should be minimal. Specification limits for endotoxins and bioburden in components and bulk solution  
117 should be provided where relevant.

118 Validation data should be provided for all the filters used in the manufacturing process of the finished  
119 dosage form. All non-sterilising filters should be validated with regards to solution compatibility and  
120 leachable filter materials, the solution to be filtered should be used in the validation unless justified.  
121 Additional validation requirements for sterilising filters are described below.

122 High bioburden limits should not be justified by the capacity of the sterilisation process or any  
123 bioburden reducing step before sterilisation.

124 If a secondary container, (e.g. secondary pouch for infusion bags or blisters intended to keep the  
125 outside of the primary package sterile), is used to provide a specific protection to the medicinal  
126 product, the packaging process should be described. Information should be provided on when the  
127 packaging is performed (before or after sterilisation), if the primary package is dry at the time of  
128 packaging and any aseptic techniques employed. The proposed routines should be justified from a  
129 microbiological perspective. If the use of secondary packaging means additional sterilisation of the  
130 drug product is performed, this should be justified with regard to sterility assurance and any potential  
131 impact on drug product quality.

#### 132 Steam sterilisation

133  $F_0 \geq 8$  minutes is required for all steam sterilisation processes. Method (e.g. saturated steam cycle,  
134 air/steam-overpressure cycle, vacuum phase), pressure, time and temperature of the sterilisation cycle  
135 and a bioburden limit should always be stated.

136 The cycle lethality, in terms of  $F_0$ , should be stated, if used as an additional control measure. The  
137 lowest temperature used to determine  $F_0$  should be stated.

138 Further information regarding the  $F_0$  concept and microbial reduction is provided in Ph. Eur. 5.1.5  
139 *Application of the  $F_0$  concept to steam sterilisation of aqueous preparations.*

140 For terminal sterilisation using a reference condition of the Ph. Eur. 5.1.1, ( $\geq 121$  °C,  $\geq 15$  min in all  
141 units), validation data for the sterilisation cycle is not required. In all other cases physical and  
142 biological validation of the sterilisation cycle should be provided, to demonstrate a SAL of  $10^{-6}$  or  
143 better, as described in Ph. Eur. 5.1.1. The SAL of such a sterilisation process should be calculated from  
144 the maximum bioburden per container.

145 If, in exceptional cases, steam sterilisation is performed with drug product temperature below 115 °C  
146 during the holding phase, this should be scientifically justified and supported by extended data, for  
147 instance, by evaluation of heat resistance for the bioburden per batch, as cycle lethality decreases  
148 significantly with decreasing temperature. Heat treatment at a temperature below 110 °C is not  
149 acceptable for sterilisation purposes.

150 Where required, sufficient validation data should be submitted to demonstrate that a SAL of not less  
151 than  $10^{-6}$  is obtained for all containers. The data should include at least, but is not limited to:

- 152 • Load mapping distribution (cold spots) – summary or confirmation of performance;
- 153 • Physical and biological cycle effect confirmation summary of at least three autoclave runs ensuring:

- 154 – Sufficient time at or above nominal temperature in the whole autoclave;
- 155 – Acceptable temperature differences between thermocouples in the load;
- 156 – Acceptable  $F_0$  variability within the load;
- 157 – Relationship between physical and biological validation.
- 158 • For processes carried out at  $\leq 115$  °C the following additional data should be provided:
- 159 – A justification for the start point of the sterilisation phase;
- 160 – Several relevant biological indicators could be included in the validation to demonstrate
- 161 sensitivity to the process.

162 For the biological validation, a biological indicator as described in Ph. Eur. chapter 5.1.2 *Biological*

163 *indicators of sterilisation* should be used.

164 A limit for bioburden should be established. For aqueous solutions, a maximum bioburden limit of

165 100 CFU/100 ml (TAMC) is acceptable for active substances, excipients and drug product formulations

166 without further justification. Other testing regimes to control bioburden at the defined level could be

167 accepted.

#### 168 Dry heat sterilisation

169 Time and temperature of the sterilisation cycle and a bioburden limit should always be stated.

170 In the case of terminal sterilisation using a reference condition of the Ph. Eur. 5.1.1, no validation data

171 of the sterilisation cycle is requested.

172 For terminal sterilisation cycles with time and/or temperature lower than the reference conditions of

173 the Ph. Eur., physical and biological validation of the sterilisation cycle should be provided, to

174 demonstrate a SAL of  $10^{-6}$  or better, as described in Ph. Eur. 5.1.1. The SAL of such a sterilisation

175 process should be calculated from the maximum bioburden per container.

176 Where required, sufficient validation data should be submitted to demonstrate that a SAL of not less

177 than  $10^{-6}$  is obtained for all containers. The data submitted should include at least, but is not limited to

- 178 • Load mapping distribution (cold spots) – summary or confirmation of performance;
- 179 • Physical and biological cycle effect confirmation summary of at least three sterilisation runs
- 180 ensuring:
- 181 – Sufficient time at or above nominal temperature in the whole dry heat sterilisation cabinet;
- 182 – Acceptable temperature differences between thermo couples in the load;
- 183 – Acceptable lethality variability within the load;
- 184 – Relationship between physical and biological validation.

185 For the biological validation, a biological indicator as described in Ph. Eur. chapter 5.1.2 *Biological*

186 *indicators of sterilisation* should be used.

187 A limit for bioburden should be established. A maximum bioburden limit of 100 CFU/100 g or ml

188 (TAMC) is acceptable for active substances, excipients and drug product formulations without further

189 justification. Other testing regimes to control bioburden at the defined level could be accepted.

190 Dry heat at temperatures of greater than 220 °C for a validated time is frequently used for both  
191 sterilisation and depyrogenation of glassware. In this case, demonstration of a 3 log reduction in heat-  
192 resistant endotoxins can be used as validation criteria.

#### 193 Ionization radiation sterilisation

194 Data as requested in Note for Guidance “The use of Ionization Radiation in the Manufacture for  
195 Medicinal Products” should be provided, supplemented as necessary by data requirements given in ISO  
196 11137 and Ph. Eur. chapter 5.1.1.

197 Where any requirements in ISO 11137 are in contradiction to requirements stated in any Note for  
198 Guidance issued by the EMA, the requirements of the Note for guidance apply.

#### 199 Gas sterilisation

200 This method provides sterilisation of the surface of the goods only. It is mainly employed for sterilising  
201 packaging materials and equipment, and has therefore not been included in the decision tree. To  
202 ensure adequate sterility, sufficient penetration by gas and moisture is essential. This should be  
203 followed by a purging process to ensure that any residues of gas or related transformation by-products  
204 are below concentrations that could give rise to toxic effects during use of the product. The  
205 effectiveness of the purging process should be demonstrated.

206 Gas sterilisation of dry powders is not acceptable unless other methods of sterilisation are not feasible  
207 and its use is scientifically justified. The substance should be sterile filtered and crystallised under  
208 aseptic conditions in order to minimise bioburden and entrapment of microorganisms within the  
209 crystals. Convincing evidence should be provided demonstrating that the product is not susceptible to  
210 compression preventing gas and moisture penetration during sterilisation.

211 A description of the apparatus, quantitative data on the mixture of gases to be used, the bioburden  
212 prior to sterilisation, the time of exposure to the gas, the temperature and humidity prior to and during  
213 each step of the sterilisation cycle, and, if applicable, the conditions for the removal of any toxic gas  
214 residues should be provided. These conditions should be monitored by appropriate in-process controls  
215 with justified acceptance limits.

216 Results of the process validation should demonstrate a SAL of  $10^{-6}$  or better and removal of any toxic  
217 gas residues to an acceptable level in line with current guidelines.

218 The effectiveness of the process should be routinely checked for every product batch using a suitable  
219 biological indicator and by product sterility testing.

220 Ethylene oxide (ETO) is a gas which is highly toxic. ETO sterilisation is only acceptable if no other  
221 method of sterilisation is possible. The process should be developed and validated according to ISO  
222 11135. Residual genotoxic impurities (for instance ETO and halogenated ethylenehydrides) should be  
223 evaluated in accordance with the requirements of ICH M7, unless the product is outside the scope of  
224 that guideline. For products outside the scope of ICH M7 the limits below apply.

225

226

<b>Material</b>	<b>Ethylene oxide</b>	<b>Ethylene chlorhydrin (or any other halogenated ethylenehydrine)</b>
<b>Raw materials</b>	1 µg/g	50 µg/g
<b>Finished product (when used on the finished product)</b>	1 µg/g	50 µg/g
<b>Container (based on simulated use)</b>	1 µg/ml	50 µg/ml

227

228 For empty containers intended to be filled with aqueous products, (e.g. prefilled syringes), the need to  
229 justify the use of ETO in the sterilisation of the container prior to filling can be waived, provided the  
230 container itself fulfils the requirements of ICH M7, as the degradation kinetics of ETO in an aqueous  
231 medium have been sufficiently demonstrated.

### 232 Sterile filtration

233 The type and number of sterilising filters, filter area, material and nominal pore size should be  
234 described together with a description of the filter integrity testing (principle of the test and details  
235 when the tests are performed including limits before and after filtration). The integrity of the sterilised  
236 filter should be verified before use but after its sterilisation unless specifically justified and validated,  
237 and should be confirmed immediately after use. Nominal pore sizes of 0.22 µm or less are acceptable  
238 without further justification, in accordance with Ph. Eur.

239 For routine commercial manufacturing, bioburden testing should be performed on the bulk solution  
240 immediately before sterile filtration. If a pre-sterilising filter is additionally installed, the filter closest to  
241 the filling point in the final container is generally characterised as the sterilising filter. The sampling for  
242 bioburden testing may be performed prior to the pre-filtration, provided that no holding time is  
243 scheduled for the solution between the two filtration steps.

244 In most situations, a limit of NMT 10 CFU/100 ml (TAMC) would be acceptable for bioburden testing. If  
245 a pre-filter is added as a precaution only and not because the unfiltered bulk solution has a higher  
246 bioburden, this limit is applicable also before the prefilter and is strongly recommended from a GMP  
247 point of view. A bioburden limit of higher than 10 CFU/100 ml before pre-filtration may be acceptable if  
248 this is due to starting material known to have high microbial contamination. In such cases, it should be  
249 demonstrated that the first filter is capable of achieving a bioburden of NMT 10 CFU/100 ml prior to the  
250 last filtration. Bioburden should be tested in a product sample of 100 ml in order to ensure the  
251 sensitivity of the method. Other testing regimes to control bioburden at the defined level could be  
252 accepted if adequately justified.

253 Filter validation data should be included. The filter should be validated with regards to bacterial  
254 retention capacity, solution compatibility and leachable filter materials. The solution to be filtered  
255 should be used in the validation unless justified, (for instance when the pre-filtration integrity test is  
256 performed using water for injections during routine production).

257 If a sterilising filter is used for more than one working day or is re-used for additional batches, the  
258 total filtration time and the number of batches the filter is used for should be stated and justified. If re-  
259 used, the filter should be dedicated to a single product and sterilised before re-use. Its integrity should  
260 be tested before and after each use. Suitable evidence of the bacterial-retention capability after

261 challenging the filter system to simulate exposure during a campaign should be provided. This  
262 simulation should include any physical handling of the filter during its use, such as maximum combined  
263 sterilisation time and temperature, integrity testing, mechanical handling and maximum filtration  
264 volume at maximum pressure.

265 The maximum holding time between bulk solution preparation and sterile filtration should be stated,  
266 minimised and appropriately supported by data.

267 If a sterile bulk solution is not filled immediately into the final product containers, the sterile filtration  
268 should, unless justified, be repeated immediately before filling in containers.

#### 269 Aseptic processing

270 Aseptic processing is not considered to be a sterilisation process as it does not reduce any  
271 microbiological contamination but only concerns techniques to process sterile components without  
272 adding any microbiological contamination.

273 For aseptic processes, information on the bulk holding time before filling and on the filling time should  
274 be stated and appropriately supported by data. The times should be minimised. The grounds for  
275 holding times longer than 24 hours should be justified and evidence should be provided demonstrating  
276 that microbial contamination is not possible during processing, (e.g. tightness of tanks, plumbing, any  
277 transportation of storage tank and storage conditions).

278 It should be confirmed that the results of the media fills support the proposed holding and filling times.  
279 The actual results of media filling fall within the field of GMP and need not be presented routinely, but  
280 may be requested by the competent authorities in certain circumstances since such data are important  
281 to justify proposed holding and filling times.

282 Sterile primary packaging materials should be used for aseptically processed products.

283 Where blow-fill-seal technology is used for aseptically processed products, summary validation data  
284 should be provided to confirm that the container produced is sterile. The bioburden of the material(s)  
285 used for the manufacture of the blow-fill-seal container should be controlled.

#### 286 **4.2. Good manufacturing practice for sterile active substances and sterile** 287 **excipients**

288 The basic GMP requirements for active substances used as starting materials (European Union (EU)  
289 GMP guide part II) only apply to the manufacture of sterile active substances up to the point  
290 immediately prior to the active substance being rendered sterile. The sterilisation and aseptic  
291 processing of sterile active substances is considered to be a step in the manufacture of the medicinal  
292 product and shall be performed in accordance with GMP for medicinal products. This implies that for  
293 any active substance manufacturer who performs sterilisation and subsequent aseptic handling of the  
294 active substance, a valid manufacturing authorisation or GMP certificate from an EEA authority or from  
295 an authority of countries where mutual recognition or other Community arrangements apply has to be  
296 submitted.

297 Similarly, for sterile excipients, any sterilisation and aseptic processing should be performed in  
298 accordance with GMP for medicinal products with the same requirements as described above for sterile  
299 active substances.

300 The same GMP and data requirements also apply to sterile active substances and excipients supported  
301 by a Certificate of Suitability issued by the EDQM.

### 302 **4.3. Selection of sterilisation method**

303 Products intended to be sterile should be terminally sterilised in their final container whenever  
304 possible, as clearly stated in the Ph. Eur., general chapter 5.1.1. When terminal sterilisation by heat is  
305 not possible, the application of an alternative method of terminal sterilisation, sterilising filtration  
306 and/or aseptic processing may be considered. It is recognised that terminal sterilisation processes  
307 utilising conditions other than the Ph. Eur. reference conditions may be developed to provide  
308 satisfactory sterility assurance levels and such alternative processes may be acceptable when properly  
309 validated.

310 If a sterilisation process using principles other than those described in the Ph. Eur. (steam, dry heat,  
311 ionising radiation, gas sterilisation and sterilising filtration) is intended to be used for the sterilisation  
312 of a product, the applicant may consider seeking scientific advice regarding the acceptability of the  
313 method and the documentation required.

314 During the manufacturer's evaluation of whether a terminal sterilisation cycle is possible, substantial  
315 efforts should be made to enable terminal sterilisation. If the active substance or some key component  
316 of the formulation is shown to degrade significantly or an impurity limit is exceeded during shelf-life  
317 under even the least stressful terminal sterilisation conditions, the efforts made to develop a  
318 formulation capable of undergoing terminal sterilisation should be presented in the development  
319 section.

320 In case of medicinal products containing highly sensitive active substances, (e.g. proteins or heat labile  
321 biological substance), where it is well known that terminal sterilisation is not possible, a justification  
322 based on a scientific rationale is generally acceptable and further justification of the choice of aseptic  
323 processing discussed later in section 4.3 may not be needed.

324 The principles for the choice of sterilisation process are presented in the form of decision trees in  
325 section 5 of this guideline.

326 For products where terminal sterilisation is not possible and aseptic processing is proposed, the  
327 decision trees should be considered to be applied to individual components of the formulation. Also,  
328 the possibility of applying a terminal microbial reduction process may be evaluated. It is emphasised  
329 that this additional microbial reduction process should not compensate for poor aseptic manufacturing  
330 practice. The same requirements for the aseptic part of the process apply as for products  
331 manufactured without such an additional microbial reduction process. In case of any non-compliance in  
332 the course of sterile filtration and/or in the aseptic manufacturing chain, decisions on whether to  
333 release batches should not rely on the terminal microbial reduction process.

334 A change in shelf-life or storage conditions caused by a terminal sterilisation process is not in itself a  
335 reason to allow aseptic processing, unless the new storage condition or shelf-life would cause problems  
336 in the use of the product.

337 Aseptic processing cannot be accepted based solely on an increase in impurity levels upon terminal  
338 sterilisation without further justification. An increased level of impurities above the ICH Q3B or VICH  
339 GL11 identification or qualification limit does not necessarily preclude terminal sterilisation of the  
340 medicinal product. The risk induced by the degradation should be balanced with the risk induced with  
341 an aseptic manufacturing method also taking in account the posology of the product and the nature of  
342 the degradation products. Attempts to find terminal sterilisation conditions adjusted to give acceptable  
343 impurity levels based on degradation mechanisms of the active substance and the actual bioburden  
344 should be described in the quality dossier.

345 In certain cases, as described in the bullet points below, the use of aseptic processing may be  
346 accepted, even if the formulation itself can be terminally sterilised. The aseptic approach should be  
347 clearly documented, explained and scientifically justified. Such cases could be justified by:

- 348 • User benefit provided by a container that cannot be terminally sterilised such as:
- 349 – Eye drop containers enabling administration of single drops to the eye;
  - 350 – Containers enabling non parenteral multi-dose preservative free medicinal product formulation  
351 for human use;
  - 352 – Enhanced ease of administration, for instance the use of a pre-filled pen compared to a vial;
  - 353 – Safer handling of toxic products, for instance plastic vials instead of glass vials for cytotoxic  
354 medicinal products.

355 The choice to use a heat-labile packaging material cannot in itself be the sole reason for not using a  
356 terminal sterilisation process and alternative materials could be examined; for instance, polypropylene  
357 is not as sensitive to heat as polyethylene and could allow terminal sterilisation. Thus, a discussion  
358 regarding the efforts made to develop a container that may be terminally sterilised should be included.

- 359 • Enabling as long a shelf-life as possible for radiopharmaceutical medicinal products with a shelf-life  
360 of less than one week.

361 The acceptability of aseptic processing should be based on the application of the decision tree and a  
362 risk assessment. The bullet points below are not intended to be used to justify aseptic processing as  
363 such, but are only intended to provide guidance on issues that are considered when evaluating the  
364 acceptability of a sterilisation or aseptic process. Considerations include (but are not limited to):

- 365 • Evidence that the proposed packaging with enhanced user benefits is fit for purpose;
- 366 • Stability of the active substance, the degradation mechanism(s) and the toxicity of impurities  
367 formed during the sterilisation process;
- 368 • The volume to be administered per dose. Large volume parenterals should be terminally sterilised  
369 whenever possible.

370 In conclusion, the justification for the chosen sterilisation or aseptic process should include a thorough  
371 benefit risk evaluation and it should be demonstrated that suitable development efforts have been  
372 made.

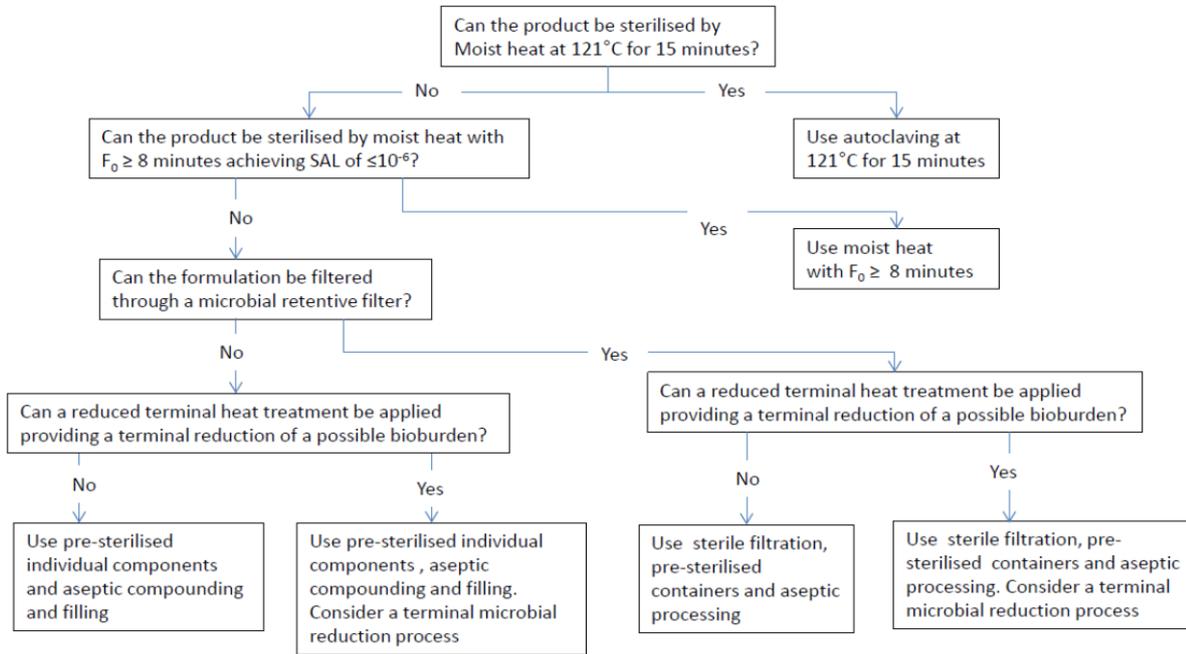
## 373 5. Decision trees

374 The decision trees are intended to assist in the selection of the optimal sterilisation method taking into  
375 account the various issues to be considered. When moving down the decision trees, the methods  
376 generally show decreasing levels of sterility assurance and therefore the first possible option should  
377 normally be chosen. The decision trees have been elaborated primarily for products containing  
378 chemical active substances, but may be applicable also to other types of products. In the case of  
379 biological products, an alternative approach may be appropriate.

380 For formulations that cannot withstand a complete terminal sterilisation cycle, a method combining  
381 aseptic processing and a terminal microbial reduction process may be considered in order to achieve a  
382 higher level of sterility assurance.

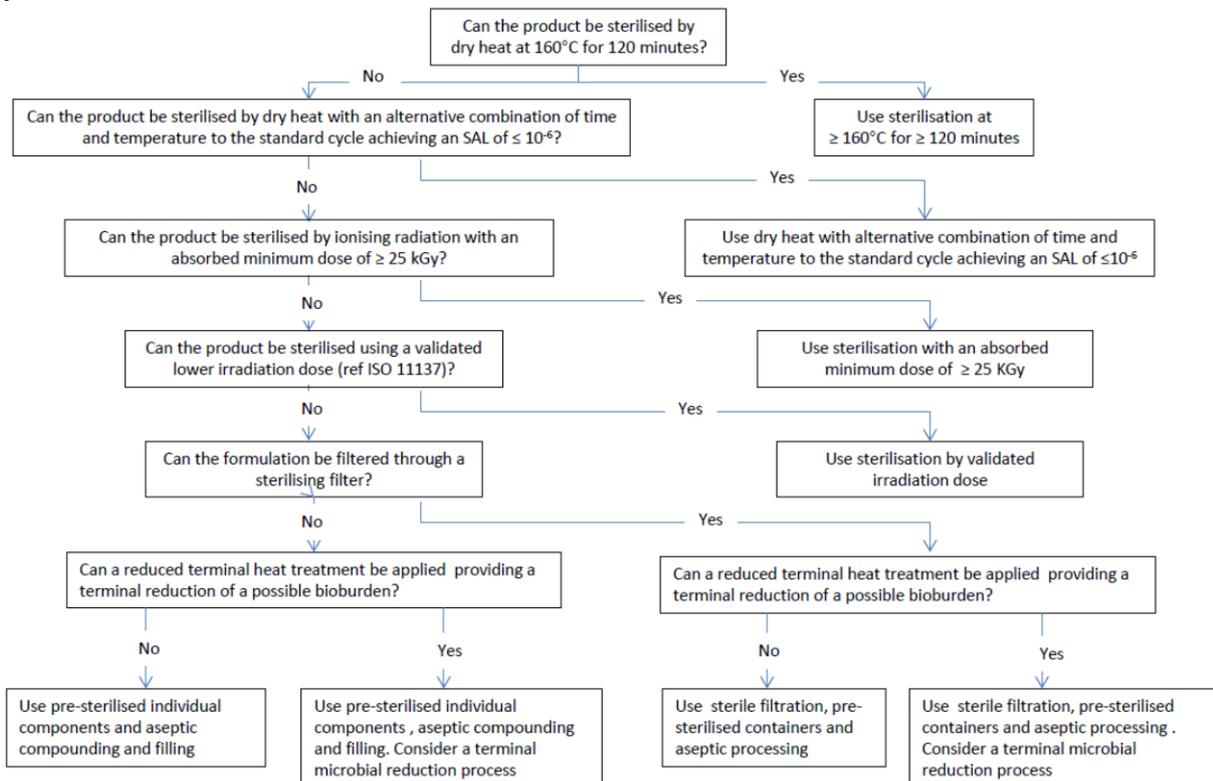
383 For solutions containing an antimicrobial preservative or inherent antimicrobial properties, the  
 384 bioburden may be more sensitive to a sterilisation process than for a non-preserved solution.  
 385 Therefore, a terminal microbial reduction process may obtain a SAL of  $\leq 10^{-6}$  and could therefore be  
 386 considered even though it would not be feasible for a preservative free product. However, the inclusion  
 387 of a preservative in a product filled in single dose containers is not accepted.

388 **Decision tree for sterilisation choices for aqueous products**



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390 **Decision tree for sterilisation choices for non-aqueous liquid, semi-solid or dry powder**  
 391 **products**



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## 394 6. Definitions

Aseptic process	<p>A process performed maintaining the sterility of a material* that is assembled from components, each of which has been sterilised by steam, dry heat, ionizing radiation, gas or sterile filtration. This is achieved by using conditions and facilities designed to prevent microbial contamination.</p> <p>* active substance, excipient, container, drug product</p>
Bioburden	<p>A population of viable microorganisms in a product prior to sterilisation</p>
Critical Quality Attribute	<p>A physical, chemical, biological or microbiological property or characteristic that should be within an appropriate limit, range, or distribution to ensure the desired product quality</p>
D-value (decimal reduction value)	<p>The value of a parameter of sterilisation (duration or absorbed dose) required to reduce the number of viable organisms to 10 per cent of the original number. It is only of significance under precisely defined experimental conditions.</p> <p><math>D_{121}</math> is the D-value of the relevant spores at 121 °C.</p>
$F_0$ value	<p>The <math>F_0</math> value of a saturated steam sterilisation process is the lethality expressed in terms of the equivalent time in minutes at a temperature of 121 °C delivered by the process to the product in its container with reference to micro-organisms possessing a theoretical Z-value of 10.</p>
Filling time	<p>The time used to fill a bulk product into containers until the container is closed or, in the case of a product which is lyophilized after the filling, until the lyophilisation chamber is closed.</p>
Holding time	<p>The time between two process steps.</p>
Large-volume parenteral	<p>An infusion or injection supplied in a container with a nominal content of more than 100 ml.</p>
Microbial reduction process	<p>Treatment at conditions that provide a lower lethality than sterilisation.</p>
Ph. Eur. sterilisation reference conditions	<p>The reference conditions for sterilisation specified in Ph. Eur. 5.1.1, i.e. terminal steam sterilisation at <math>\geq 121</math> °C for 15 min, terminal dry heat sterilisation at <math>\geq 160</math> °C for <math>\geq 2</math> h or terminal</p>

	ionising radiation of 25 kGy.
SAL	Sterility Assurance Level. The SAL of a sterilising process is the degree of assurance with which the process in question renders a population of items sterile. The SAL for a given process is expressed as the probability of a non-sterile item in that population. An SAL of $10^{-6}$ , for example, denotes a probability of not more than one viable micro-organism in $1 \times 10^6$ sterilised items of the final product.
Sterilisation	A process that inactivates or removes viable micro-organisms in a product until sterility is obtained.
Sterility	Absence of viable micro-organisms. The inactivation of micro-organisms by physical or chemical means follows an exponential law; thus there is always a finite statistical probability that a micro-organism may survive the sterilising process. For a given process, the probability of survival is determined by the number, types and resistance of the micro-organisms present and by the environment in which the organisms exist during treatment.
TAMC	<i>Total aerobic microbial count:</i> The total aerobic microbial count (TAMC) is considered to be equal to the number of CFU found using casein soya bean digest agar.
Terminal microbial reduction process (of product)	Microbial reduction process (of product) in the final container
Terminal sterilisation (of product)	Sterilisation (of a product) in its primary container
Validation	The action of proving, in accordance with the principles of GMP, that any procedure, process, equipment, material, activity or system actually leads to the expected results.
Z-value	The Z-value is the change in temperature required to alter the D-value by a factor of 10.

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## 397 7. References

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400 the selection of sterilisation methods, EMEA/CVMP/065/99;
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- 403 ICH guideline Q8 (R2) on pharmaceutical development, EMA/CHMP/ICH/167058/2004;
- 404 European Pharmacopoeia general chapter 5.1.1 'Methods of preparation of sterile products';
- 405 Directive 2001/83/EC of the European Parliament and of the Council of 6 November 2001 on the  
406 Community code relating to medicinal products for human use;
- 407 Directive 2001/82/EC of the European Parliament and of the Council of 6 November 2001 on the  
408 Community code relating to veterinary medicinal products;
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- 410 Guideline on Manufacture of the Finished Dosage Form (CPMP/QWP/486/95 and  
411 EMA/CHMP/QWP/245074/2015);
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413 EMA/CHMP/QWP/811210/2009-Rev1;
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- 420 ICH guideline M7 on assessment and control of DNA reactive (mutagenic) impurities in pharmaceuticals  
421 to limit potential carcinogenic risk (EMA/CHMP/ICH/83812/2013);
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- 424 VICH Topic GL11 Guideline on impurities in new veterinary medicinal products,  
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